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Performance and Effectiveness of a Passive Back support Exoskeleton in Manual Material Handling Tasks in the Construction Industry

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6 Abstract

7 Work-related musculoskeletal disorders are a leading contributor to workplace injuries in the 8 construction industry, with the low back being the most affected body part. Recent 9 developments have led to the introduction of exoskeletons on industrial job sites as a means to mitigate the risk of work-related musculoskeletal disorders. Due to the newness of industrial 10 exoskeletons, the successful application of this technology in the construction industry requires 11 a thorough evaluation of different aspects of its adoption, especially user acceptance, to ensure 12 a successful and effective uptake. As manual material handling tasks are the most common cause 13 14 of low back injuries, this study aimed to evaluate the impact of using exoskeletons when adopting 15 different postures during dynamic and static manual material handling tasks. An experiment was carried out and data reflecting Rate of Perceived Exertion, Level of Discomfort, overall fit and 16 comfort, effectiveness, and interference levels were collected. Overall, the participants perceived 17 18 the exoskeleton suit as effective, with discomfort being reduced in the low back and most other body parts. However, the results indicated the importance of considering the specific task at hand 19 (e.g., dynamic vs static manual material handling) and the posture adopted (e.g., squatting vs 20 21 stooping) when evaluating and selecting an exoskeleton for construction tasks. Also, the results

show differences between male and female participants in most usability and effectiveness responses. In conclusion, passive exoskeletons have the potential to be adopted to reduce the rate of WMSDs in construction. However, proper training and supervision are required on the postures adopted by the workers, based on the specific characteristics of the task carried out. Also, different results from male and female responses show that different exoskeletons, or an exoskeleton with two different designs, may lead to higher efficiency than using one exoskeleton for both groups.

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30 Keywords: Exoskeleton; Back-support; Manual Material Handling; Construction; Ergonomics;
 31 Wearable robot

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- 34

35 **1- Introduction**

36 Work-related Musculoskeletal Disorders (WMSDs) are the most common and fastest increasing 37 cause of work-related disabilities [1, 2]. If not treated properly, these disorders can impose 38 substantial costs [1]. In Europe, WMSDs are the most common cause of disability, absence, and 39 loss of productivity [3]. Work that involves heavy lifting, awkward postures, and repetitive 40 movements are among the most common biomechanical factors associated with WMSDs [4]. In 41 the construction industry, manual material handling (MMH) involving lifting, carrying, pushing, 42 pulling, lowering, restraining, and holding is the most common cause of occupational fatigue, low 43 back pain and injuries. Both dynamic (e.g. carrying) and static (e.g. holding) MMH tasks can lead 44 to high rates of WMSDs, including 30% of all lost workday cases among construction trades in the 45 US [5].

46 In addition to job and workplace ergonomics training, technical interventions are one of the most 47 effective mitigation strategies when it comes to preventing WMSDs [6]. An easy-to-implement 48 wearable assistive device called an exoskeleton, also known as exosuits or wearable robots, can 49 reduce fatigue and strain, thereby preventing injuries to those parts of the body that are stressed 50 the most during everyday workplace activities [7-10]. Recently, these wearable robots are 51 adopted for different industrial applications to mitigate the ergonomic risks associated with 52 physically demanding tasks, especially the ones involving MMH. The use of exoskeletons for such 53 physically demanding tasks has shown to reduce fatigue and the frequency of injuries [11]. 54 Considering the complex nature of construction tasks and the fact that WMSDs are 55 disproportionately prevalent among construction workers [9], exoskeletons may be a particularly 56 effective and novel control method to mitigate WMSDs in this industry.

In a recent study, Zhu et al. [12] investigated existing exoskeleton technologies and analyzed their potential for MMH tasks in construction. They generated a map to suggest the appropriate exoskeleton type for each trade while evaluating the benefits and challenges. In another study, Cho et al. [13] designed a wearable exoskeleton to habituate construction workers to safe postures and demonstrated that the developed exoskeleton can effectively assist workers when performing construction tasks. Ogunseiju et al. [14] evaluated a postural assist exoskeleton and its effectiveness for construction tasks involving MMH. They reported improvements in posture 64 when using the exoskeleton over time, although higher perceived discomfort in the low back was 65 reported due to the pressure applied to the users' back. In another study, Capitani et al. [15] 66 described the development of a passive exoskeleton to assist construction workers in dealing 67 with shotcrete projection tasks. They indicated that the designed exoskeleton preserved 68 adaptability to different lower-limb tasks without reducing its comfort during utilization. 69 Furthermore, Chen et al. [16] presented a bilateral knee exoskeleton to provide kneeling 70 assistance for construction workers. The results showed reductions in knee pressure, potentially 71 leading to decreased WMSD risk for workers when performing kneeling activities on level and 72 sloped surfaces.

73 In previous studies, it is shown that the effectiveness of the exoskeletons depends heavily on 74 user acceptance since exoskeletons use may present unexpected safety and usability challenges 75 [9, 17]. Thus, more research is required to evaluate the different usability aspects of the adoption 76 due to the recentness of using the exoskeleton technology for the construction industry. Also, 77 most of the previous studies have focused on a limited types of MMH tasks in terms of their 78 nature (static, dynamic) and body posture (e.g. squatting, bending), while there are various types 79 of MMH tasks in the construction industry, and there is a lack of studies around these tasks, 80 especially for the construction sector. Considering these points, this study aimed to evaluate the 81 effect of a back-support exoskeleton on postures adopted when carrying out construction MMH 82 tasks. The goal of this study was to compare different postures, squatting and bending, adopted 83 during dynamic and static MMH tasks, with and without exoskeletons. The experiments were 84 designed to provide feedback on the impact of using exoskeletons on comfort, fatigue, load 85 distribution, worker' intention-to-use, and other usability factors. Both male and female subjects 86 were considered since the effectiveness of exoskeletons was not well-studied in terms of gender 87 differences in the previous studies.

88 2- Material and Methods

89 2-1- Experimental design

We used a passive exoskeleton for the experiment, since passive exoskeletons have shown to be
more suitable for a number of industrial applications compared to active exoskeletons due to

92 lighter weight, lower price and simpler maintenance [5]. Furthermore, we studied a back-support 93 exoskeleton, since the back is the primary body part affected by WMSDs in construction. Back 94 support exoskeletons are designed to reduce the load on the low back muscles during bending 95 tasks by redistributing the weight to the legs [18]. We used a BackX exoskeleton which weighs 96 7.2 lbs and can reduce the strain on the user's low back. It consists of two leg straps and a vest 97 coupled to each other by two torque generators at both hip joints. Also, it has two operation 98 mode, instant and standard. In the instant mode, it is engaged in all postures, while in standard 99 mode, support is provided when the users' trunk bends 30° to 45°. We selected this exoskeleton 100 because it can be used for a variety of MMH tasks, such as bending, squatting, walking. It is shown 101 that BackX can minimize the risk of back injuries among workers who repeatedly go through 102 stooping, squatting, and bending postures for various tasks [18]. The experiment was designed 103 to simulate dynamic and static MMH tasks. Participants were asked to carry out the tasks in 104 different scenarios to cover different task types (i.e., dynamic and static), postures (i.e., freestyle, 105 bending, squatting), and the impact of the exoskeleton (i.e., with and without wearing the 106 exoskeleton).

107 **2-2- Participants**

For this study, 12 able-bodied individuals, including 6 male and 6 female, were asked to participate in the experiment. The mean and standard deviation for the age, body weight, and body height of the participants were 28 ± 6.28 years old, 64.8 ± 15.4 kg, and 1.7 ± 0.1 m, respectively. None of the participants reported any current or previous musculoskeletal disorders or illnesses. The detailed process including the objectives, instructions and possible risks were explained to each participant through written and verbal instructions and on-site discussions. Ethics approval was received for the study from the University of Alberta Research Ethics Board.

115 **2-3- Testing Procedure**

The variables of the experiment included freestyle, bending, and squatting lifting postures, existence of the exoskeleton, and the static and dynamic nature of the task. Dynamic MMH involved lifting a 20 lb. box, carrying it during a 32-foot walking , and placing it and the floor for five times, while each time lifting and placing on a surface with a different height (i.e., on the floor and on a table). Static MMH tasks involved moving items, with weight less than 0.5 kg, from
a box and placing them on a table through a static posture.

122 Prior to the experiment, participants were introduced to the procedure and equipment. 123 Participants were given enough time between every two experimental trials to recover from any 124 fatigue associated with performing the task. After completing each trial, the participants were asked a series of questions including the Rate of Perceived Exertion (RPE), Level of Discomfort 125 126 (LOD), overall fit and comfort of using the exoskeleton, the extent to which the exoskeleton 127 limited movements and interferes with movements, effectiveness of the exoskeleton, and other 128 general feedback. In total, seven scenarios reflecting different postures and the exoskeleton's 129 use were tested. Fig. 1 also shows the experiment setup for some of the scenarios as a sample.

130 **2-4- Participant Response**

131 The participants were asked to rate the level of their perceived discomfort (i.e., LOD) on a Borg 132 CR 10 scale, where 0 indicates no discomfort and 10 shows maximum discomfort [19]. The 133 intensity of perceived discomfort was measured and quantified after conducting each 134 experimental trial. Furthermore, the participants provided the discomfort ratings separately for 135 each body part including shoulder, chest, low back, thighs, feet, etc. on a scale of 0 to 10. Also, 136 RPE was rated from 1 (very light activity) to 10 (maximum effort), fit/comfort of the exoskeleton 137 suit was rated from 1 (not satisfactory) to 10 (very satisfactory), limitation/interference was rated 138 from 1 (limits a lot) to 10 (does not limit at all), and effectives was rated from 1 (not effective at 139 all) to 10 (very effective). Collected data was explored through descriptive statistical analysis.

140 **3- Results**

141 **3-1- Dynamic tasks**

According to Fig. 2, the average RPEs for the different posture scenarios during the dynamic MMH were fairly close. Overall, it can be concluded that the exoskeleton's use and the posture used does not impact the average RPE in dynamic MMH. It is also worth noting that in cases where the exoskeleton was used, a maximum RPE of 6 was reported by users.

146 The results indicate that the participants felt similar effectiveness in all postures, while they 147 experienced more comfort during squatting compared to bending (Fig. 3). Overall, the participants felt that the exoskeleton moderately limits their movements and interfered withother tasks.

150 As shown in Fig. 4, most of the perceived discomfort was detected in the low back and legs. While 151 using the exoskeleton substantially reduced the discomfort in the low back during bending and 152 squatting, using the exoskeleton with a freestyle posture did not have considerable impact in 153 improving the discomfort in the low back. It is also observed that the perceived discomfort in legs 154 and arms was much higher when squatting compared to bending. The reason for this observation 155 could be mainly due to the moment tolerated by the legs and knee joints because of the weight 156 of the upper body and its considerable moment arm in squatting. Also, because of the difference 157 postures of arms during bending and squatting, the users experienced more discomfort in this 158 part of body in the squatting than bending. Fig. 4 shows an increased level of discomfort in the 159 upper leg and knee since the exoskeleton transferred load from the chest and upper body to 160 upper legs.

161 **3-2- Static tasks**

While minimum and maximum reported RPEs were similar for all scenarios, the average RPE was reported as slightly higher for squatting, which indicates the difficulty of performing the static task in a squatting posture due to the pressure applied to the legs and the need to maintain balance (Fig. 5).

As shown in Fig. 6, the overall effectiveness, interference, and comfort levels were higher inbending compared to squatting both when an exoskeleton was worn.

168 Since the body was positioned in an awkward position for a prolonged period of time during the 169 static task, the discomfort levels were generally high during static MMH tasks without the 170 exoskeleton (Fig. 7). Similar to the dynamic tasks, most of the reported discomforts were in the 171 low back and legs. The use of the exoskeleton caused higher discomfort levels on the chest during 172 bending, which was due to the chest pad. While the use of the exoskeleton reduced the 173 discomfort on the legs in bending compared to squatting, the discomfort in the low back was 174 much less in squatting. The moment arm and the weight of the upper body could be the main 175 reasons for these different observations in bending and squatting. Also, similar to the dynamic

tasks, the upper leg was negatively affected by using the exoskeleton in both bending andsquatting postures.

3-3- Dynamic MMH tasks vs. Static MMH tasks

While other factors remained the same, a higher level of limitation was reported during static tasks (Fig. 8). Overall, it can be concluded that the exoskeleton's performance for bending is similar for both static and dynamic tasks.

According to Fig. 9, the overall effectiveness, limitation and comfort levels were higher for dynamic squatting task, compared to static squatting tasks. Since dynamic tasks involve more movements, such as walking during carrying the load, it seems that the exoskeleton needs modifications to not restrict other movements than the lifting.

186 **3-4- Male vs. Female Users**

As shown in Fig. 10, male participants reported higher RPE levels in the dynamic scenarios compared to female participants. Also, the perceived exertion was similar for bending and squatting postures among both groups.

While both male and female participants reported a slightly higher RPE in squatting compared to
bending, male participants reported higher RPEs for all scenarios of static MMH (Fig. 11). Using
the exoskeleton did not improve the exertion levels when adopting the bending posture.

Table 1 shows a comparison of the average responses for the usability factors for male and female participants. As shown in Table 1, female participants found the exoskeleton more effective in all MMH scenarios, while both groups rated the fit and comfort level similar. On the other hand, female participants rated the limitation factor of the exoskeleton higher than male participants.

Male participants reported higher discomfort when carrying out the dynamic task without the exoskeleton, with the highest discomfort in the low back (Table 2). When using the exoskeleton with a freestyle posture, both male and female groups reported discomfort in the chest area, with male participants reporting substantially higher LOD. During dynamic bending, male participants reported the highest discomfort on the chest, low back, and knees, while female participants reported the highest LOD on the upper leg and knees. The highest reported LOD during dynamic squatting was felt on the chest, low back, and knees for male participants and upper leg, knees, and arms for female participants. While male participants reported discomfort
 on the shoulder in all dynamic scenarios, there was no reported LOD for shoulders by female
 participants. Overall, male participants reported higher LOD for all body parts except arms.

208 Also, when carrying out the static task without the exoskeleton, male participants reported the 209 highest discomfort in the low back, shoulder, and knees, while female participants reported the 210 highest LOD on the arms and knees. The exoskeleton's use for the static bending task resulted in 211 higher discomfort in both groups, with male participants reporting the highest LOD on the chest, 212 low back, and knees, and female participants reporting the highest LOD on the upper leg, knees, 213 and arms. For static squatting, male participants reported higher LOD in all body parts compared 214 to female participants. The highest LOD was reported in the chest, low back, and knees for male 215 participants, while the highest LOD was reported in the upper leg, knees, and arms for female 216 participants. Both groups reported similar LOD in the upper legs. Overall, similar to the dynamic 217 MMH scenarios, male participants reported higher LOD compared to female participants for all 218 body parts except arms for static MMH scenarios.

219 **3-5- User Feedback**

220 Participants were also asked for feedback on different usability metrics of the exoskeleton in an 221 open-ended format. According to Table 3, their opinion about the exoskeleton is moderate, 222 based on their overall feeling. Based on their explanations, the exoskeleton helped with 223 distributing the loads, but it also limited their movement and caused discomfort in body parts, 224 such as the chest and thigh. The level of heat/humidity that the exoskeleton caused was 225 considered ignorable by the participants. Most participants preferred to use the exoskeletons if 226 they had to do a lot of MMH tasks because although it restricted their movement, its help during 227 lifting and carrying the loads was considerable. In terms of the preferred posture, most 228 participants preferred squatting during dynamic MMH and bending during static MMH.

3-6- Combined Scenarios and Postures

Construction workers are typically involved in a variety of tasks involving both dynamic and static
 MMH as well as various postures (e.g., squatting and bending) during their daily activities. Thus,
 the combined results for different scenarios of MMH tasks can help further evaluate the
 performance of exoskeletons for tasks involving a variety of MMH tasks and postures. According

to Table 4, the average RPE did not improve when using the exoskeleton, and the RPE was higher during squatting MMH tasks compared with bending MMH tasks. Also, the exoskeleton decreased the LOD in the knee and low back. However, squatting and bending postures resulted in different LODs with exoskeleton; the LOD in the knee, arm, and shoulder parts decreased during bending MMH tasks, while the LOD in the shoulder and low back areas decreased during squatting MMH tasks.

240 **4- Discussion**

WMSDs are leading cause of loss of productivity in the construction industry, and recently exoskeletons have been proposed and used to reduce the load on workers' body parts. In this study, a passive exoskeleton (BackX) was used while doing MMH tasks. Both dynamic and static tasks as well as male and female paticipants were considered for the experiments. The results showed improvements in reducing the loads of users' body parts, especially low back, and therefore they could be adopted in the construction industry, alghouth improvements should be considered for the future designs.

248 **4-1- Static MMH Tasks**

249 In static MMH tasks, participants reported different and contradictory results in bending and 250 squatting scenarios. In terms of effectiveness and overall LOD, their opinion is more positive 251 about the bending MMH tasks, while they felt less discomfort in low back and chest in squatting 252 MMH tasks (Fig. 6). Also, in squatting, the knee was adversely affected by using the exoskeleton 253 more than other body parts, while its LOD in bending was lower than when the exoskeleton was 254 not used (Fig. 7). The reason may rely on the mechanism of each task; in the bending tasks, the 255 knee did not bear much joint moment, while in squatting, there was large joint moment due to 256 the weight of upper body and upper leg. This should be taken into consideration for future 257 modification of the exoskeletons.

258 4-2- Dynamic MMH Tasks

Participant's opinion about wearing the exoskeleton in dynamic MMH tasks was moderate.
Although the exoskeleton helps them for lifting, its use led to moderate discomfort as well. The
reason may rely on the fact that dynamic MMH tasks involved other movements, e.g., walking,

as well, and the exoskeletons may not be properly designed for those movements. Similar to
static MMH tasks, knee and upper leg were adversely affected by using the exoskeleton in
squatting (Fig. 4), highlighting the necessity of exoskeleton modification if squatting is involved.
Also, using the exoskeleton with freestyle movement is not as effective as squatting and bending,
especially in the low back.

267 **4-3- Perceived Discomfort**

268 Based on the users' perceived discomfort, the exoskeleton reduced the load, in the low back, 269 especially in squatting tasks (Table 4), and increased it in other body parts, especially the chest. 270 Also, the female participants felt less discomfort in the low back (and many other body parts) 271 than the male ones (Table 2). Kazerooni et al. [18] evaluated the BackX exoskeleton using 272 objective metrics. While their study showed that the average muscle activities of thoracic and 273 lumbar erector spinae muscles reduced 75% and 56% respectively, no significant difference 274 between male and female was found. Also, another study [20] showed that using BackX 275 exoskeletons resulted in the reduction of the peak muscle activity of lumbar erector spinae by 276 21.8% in a dynamic lifting task. These different, and in some cases contradictory, results reveal 277 two important points: (1) anthropometric differences can result in different outcomes; (2) 278 conditions of different tasks in the literature may differ and cause deviations. Thus, there is a 279 need for comprehensive studies comparing the the effect of different factors for the same study 280 participants and tasks to better understand the effect of each factor.

281 **4-4- Users' Movement**

282 Wearing exoskeleton reduced the participants' movement and resulted in feeling discomfort in 283 body parts, especially legs and chest. The results from previous studies also showed that the 284 range of motion reduced while using the exoskeletons [14, 21]. However, there was a perception 285 of benefits and willingness for users to use exoskeletons in their long-term activities (Table 3). 286 The perceived discomfort in chest and legs was expected since the torso weight was mainly 287 supported by the chest pad and straps connected to it, and also the exoskelton transferred a 288 portion of chest load to the upper-legs. However, in the future designs, it would be worth to 289 modify the exoskeleton to reduce the discomfort as it could impact the long-term user 290 compliance.

291 **4-5- Static MMH Tasks vs Dynamic MMH Tasks**

292 Comparing static and dynamic MMH tasks, the difference was not high, and in most evaluations, 293 their results were similar. Nevertheless, the results from other studies indicated differences 294 between dynamic and static MMH tasks [17, 22]. Their results showed significantly higher 295 discomfort in dynamic MMH tasks compared to static tasks. Independent of exoskeleton design 296 and test conditions, dynamic MMH tasks involve more movements, e.g. walking, than static ones. 297 Therefore, movement restriction and discomfort in dynamic MMH tasks would be higher than, 298 or at least at the level of, static MMH tasks.

299 4-6- Squatting MMH Tasks vs Bending MMH Tasks

300 The combined (e.g. considering bending from both dynamic and static tasks together) results, 301 Table 4, showed that squatting and bending tasks had different effects on participants' 302 discomfort. For example, the LOD of the low back for bending tasks (the average of its mixed 303 result) was higher than squatting tasks. Similarly, Baltrusch et al. [23] have found that the LOD 304 was higher when the task required hip flexion. Their results showed that using different 305 exoskeletons specifically adjusted for bending and squatting could result in higher effectiveness. 306 This idea was also suggested in [24], where the effect of two exoskeletons were evaluated on 307 lifting tasks.

308 **4-7- Body parts**

Using the exoskeleton increased the LOD on the chest and upper legs in all conditions. The LOD increased in chest area because of the exoskeleton's chest pad; also, since load transferring frames of the exoskeleton connect upper body to the thigh parts, the LOD in these parts is higher in all conditions of using the exoskeleton. Also, the knee and arm experienced higher LOD in squatting compared to bending, while the LOD of the low back was higher in bending. The reason, as explained in the previous sections, was due to the different postures and the moment arm of the participants' upper body weight.

316 **4-8- Male Users and Female Users**

The male and female participants reported different RPE and LOD of body parts. The female participants experienced lower RPE and LODs for most of their body parts and scenarios (Table

319 2). Alemi et al. [24] studied the effect of two exoskeletons, namely BackX and Laevo. Their results 320 for BackX exoskeleton showed that the RPE of different body parts of female participants was 321 slightly higher or equal to male participants'. Also, the normalized peak values of EMG signal 322 amplitudes for female participants were slightly higher than male participants' for all studied 323 muscles. Additionally, their results indicated that Laevo and BackX exoskeletons could be the most helpful for female and male users, respectively. Therefore, it seems that both 324 325 anthropometric differences and exoskeleton designs can led to different outcomes between 326 male and female users, and further studies are required to evaluate the effect of each factor on 327 the exoskeleton effectiveness.

328 **4-9- Future Improvements**

329 Considering all these factors and results, the examined exoskeletons should be modified in some 330 tasks to have higher effectiveness. Since the real-world users of the exoskeletons usually perform 331 movements other than those the exoskeleton is designed for, if the exoskeleton has negative 332 effects on those tasks, its usability will diminish by the time. In future designs and modifications, 333 it should be considered that using the exoskeleton should not impair the users' movements, 334 other than the targeted ones, such as walking during dynamic tasks, or body rotations during 335 static ones. In addition, exoskeletons should be adjusted to different anthropometric factors, 336 especially gender. It may result in higher performance and effectiveness if more than one 337 different sizes of exoskeleton be used with male and female users (or other anthropometricbased classifications). 338

339 **5- Evaluation Framework**

There are many exoskeletons for different MMH tasks conducted in the construction industry, but there is a lack of a standard evaluation framework for finding most appropriate exoskeleton(s) for specific task and joints. Based on the results obtained in this study together with other relevant studies in the literature, the following steps should be taken as a framework for the evaluation of the exoskeletons:

Identifying existing, commercially available exoskeletons for the targeted tasks and body
 parts.

Conducting preliminary studies to find the more appropriate exoskeletons based on
 subjective evaluations. Such metrics as the fitness, effectiveness, restriction, comfortability,
 and perceived exertion can be used in this step. The exoskeletons would be worn by a number
 of users for some days during performing their tasks. In this step, the inclusion of all
 anthropometric ranges (gender, body shape, etc) is highly valuable.

• Filling out a questionnaire at the end of each trial (collecting subjective evaluations)

- Conducting a comprehensive analysis on subjective evaluations to find the most appropriate,
 comfortable, and effective exoskeleton(s) for each gender, task, and body part. In one study
 [24], it was shown that male and females users preferred different exoskeletons for lifting
 tasks. Also, in this study, the results indicated that the effectiveness of BackX exoskeleton
 was different for male and female participants.
- Evaluation of selected exoskeletons using objective metrics. In addition to subjective
 evaluations, quantitative analysis is required to confirm the performance of the selected
 exoskeletons. Muscle activation, joint angles, and tissue loads can be studied in this step.
- Using the selected exoskeletons in the real field for a limited number of users and evaluating
 the performance of the exoskeletons based on feedback from the users .

• Using the finalized exoskeletons in long-term trials.

364

365 6- Conclusion

366 Emerging technologies, such as exoskeletons, have the potential to reduce the high rate of 367 WMSDs in the construction industry. However, their adoption has to be evaluated from different 368 aspects before introducing them to job sites, to ensure a successful and effective uptake. As 369 MMH tasks are among the top contributors to WMSDs in construction, this study aimed to 370 evaluate the impact of a passive back-support exoskeleton on different MMH task and postures. 371 The results indicate that (1) the impact of using the exoskeleton is similar for dynamic and static 372 MMH tasks, while it is slightly less effective for squatting during static tasks, (2) using the 373 exoskeleton reduces the load on the low back overall, but might cause discomfort on chest and 374 legs based on posture, (3) male participants experience higher discomfort on almost all body 375 parts when wearing the exoskeleton compared to female participants, and (4) a majority of the 376 participants rated the exoskeleton as providing acceptable usability, while female participants 377 found the suit more effective. According to the reported LOD, the low back, knees, upper legs, 378 and chest are the most affected body parts by the exoskeleton. Meanwhile, the use of 379 exoskeleton reduced discomfort in the mentioned body parts except the chest. Based on the 380 results, it can be concluded that passive exoskeletons have the potential to be adopted to reduce 381 the rate of WMSDs in construction. However, proper training and supervision is required on the 382 postures adopted by the workers, based on the specific characteristics of the task carried out. It 383 is important that exoskeletons are properly selected for the task at hand and are solely used for 384 the identified task. This study was limited to the experiments carried out for a short period of 385 time. Long-term trials are required to reflect on the impact of using exoskeletons over time. 386 Furthermore, while subjective metrics can be useful for evaluation of exoskeletons from a 387 usability perspective, the lack of objective measures limits the generalization of the analysis. 388 Future studies should also include objective evaluation features [25] for a more comprehensive 389 analysis. Furthermore, the findings of studies such as this one can be used in future studies to 390 assist with improving the design of exoskeletons.

392 **Declarations**

393 Competing interests

394 The authors declare no competing interests.

395 **Conflict of interest**

396 On behalf of all authors, the corresponding author states that there is no conflict of interest.

397 Ethics Approval

- 398 This study was approved by the research ethics board of the authors' current institution
- 399 (Pro00109264), and all methods were performed in accordance with the relevant guidelines and
- 400 regulations. All participants were informed of the experimental procedures and gave informed
- 401 written consent before the test.

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7- Tables

Table 1 Comparison of usability responses between male and female participants

Metric	Category	Trial type	Female (ave)	Female (sum)	Male (ave)	Male (sum)
Fit/Comfort	Dynamic MMH	Exoskeleton + Freestyle	6	36	6.83	41
		Exoskeleton + Bending	5.5	33	5.83	35
		Exoskeleton + Squatting	6.17	37	6	36
	Static	Exoskeleton + Bending	5.83	35	5.83	35
	MMH	Exoskeleton + Squatting	5.5	33	5.67	34
Limit/Interference		Exoskeleton + Freestyle	6.33	38	5.33	32
	Dynamic	Exoskeleton + Bending	5.17	31	5.17	31
	MMH	Exoskeleton + Squatting	6	36	5	32
	Static	Exoskeleton + Bending	6.83	41	5.33	32
	MMH	Exoskeleton + Squatting	4.83	29	5	30
	Dynamic MMH	Exoskeleton + Freestyle	6.83	41	5.67	34
		Exoskeleton + Bending	6.67	40	6.17	37
Effectiveness		Exoskeleton + Squatting	7.17	43	5.33	32
	Static	Exoskeleton + Bending	7.17	43	5.83	35
	MMH	Exoskeleton + Squatting	5.83	35	4.67	28
_	• •		Female	Female	Male	Male
	• •	- • • •	remale	remale	wale	iviale
Metric	Category	Trial type	(ave)	(sum)	(ave)	(sum
Metric		Trial type Exoskeleton + Freestyle				
Metric	Dynamic		(ave)	(sum)	(ave)	(sum
Metric Fit/Comfort		Exoskeleton + Freestyle	(ave) 6	(sum) 36	(ave) 6.83	(sum 41
	Dynamic	Exoskeleton + Freestyle Exoskeleton + Bending	(ave) 6 5.5	(sum) 36 33	(ave) 6.83 5.83	(sum 41 35
	Dynamic MMH	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting	(ave) 6 5.5 6.17	(sum) 36 33 37	(ave) 6.83 5.83 6	(sum 41 35 36
	Dynamic MMH Static MMH	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending	(ave) 6 5.5 6.17 5.83	(sum) 36 33 37 35	(ave) 6.83 5.83 6 5.83	(sum 41 35 36 35
	Dynamic MMH Static MMH Dynamic	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting	(ave) 6 5.5 6.17 5.83 5.5	(sum) 36 33 37 35 33	(ave) 6.83 5.83 6 5.83 5.67	(sum 41 35 36 35 34
	Dynamic MMH Static MMH	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Freestyle	(ave) 6 5.5 6.17 5.83 5.5 6.33	(sum) 36 33 37 35 33 38	(ave) 6.83 5.83 6 5.83 5.67 5.33	(sum 41 35 36 35 34 32
Fit/Comfort	Dynamic MMH Static MMH Dynamic	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Bending	(ave) 6 5.5 6.17 5.83 5.5 6.33 5.17	(sum) 36 33 37 35 33 38 31	(ave) 6.83 5.83 6 5.83 5.67 5.33 5.17	(sum 41 35 36 35 34 32 31
Fit/Comfort	Dynamic MMH Static MMH Dynamic MMH	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending	(ave) 6 5.5 6.17 5.83 5.5 6.33 5.17 6	(sum) 36 33 37 35 33 38 38 31 36	(ave) 6.83 5.83 6 5.83 5.67 5.33 5.17 5	(sum 41 35 36 35 34 32 31 32
Fit/Comfort	Dynamic MMH Static MMH Dynamic MMH Static MMH	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting	(ave) 6 5.5 6.17 5.83 5.5 6.33 5.17 6 6	(sum) 36 33 37 35 33 38 31 36 41	(ave) 6.83 5.83 5.83 5.67 5.33 5.17 5 5.33	(sum 41 35 36 35 34 32 31 32 32
Fit/Comfort	Dynamic MMH Static MMH Dynamic MMH Static MMH Dynamic	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Squatting Exoskeleton + Squatting	(ave) 6 5.5 6.17 5.83 5.5 6.33 5.17 6 6 6.83 4.83 6.83	(sum) 36 33 37 35 33 38 31 36 41 29	(ave) 6.83 5.83 6 5.83 5.67 5.33 5.17 5 5.33 5.33 5.33	(sum 41 35 36 35 34 32 31 32 32 30
Fit/Comfort	Dynamic MMH Static MMH Dynamic MMH Static MMH	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Squatting Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Freestyle Exoskeleton + Bending	(ave) 6 5.5 6.17 5.83 5.5 6.33 5.17 6 6 6.83 4.83 6.83 6.67	(sum) 36 33 37 35 33 38 31 36 41 29 41	(ave) 6.83 5.83 5.67 5.33 5.17 5 5.33 5 5.67 6.17	(sum 41 35 36 35 34 32 31 32 32 30 34
Fit/Comfort Limit/Interference	Dynamic MMH Static MMH Dynamic MMH Static MMH Dynamic	Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Freestyle Exoskeleton + Bending Exoskeleton + Squatting Exoskeleton + Squatting Exoskeleton + Squatting	(ave) 6 5.5 6.17 5.83 5.5 6.33 5.17 6 6 6.83 4.83 6.83	(sum) 36 33 37 35 33 38 31 36 41 29 41 40	(ave) 6.83 5.83 5.67 5.33 5.17 5 5.33 5.17 5 5.33 5.17	(sum 41 35 36 35 34 32 31 32 32 30 34 37

477	Table 2 Comparison of LODs between male and female participants
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Metric	Category	Trial type	Female (ave)	Female (sum)	Male (ave)	Male (sum)
Fit/Comfort	Dynamic MMH	Exoskeleton + Freestyle	6	36	6.83	41
		Exoskeleton + Bending	5.5	33	5.83	35
		Exoskeleton + Squatting	6.17	37	6	36
	Static	Exoskeleton + Bending	5.83	35	5.83	35
	MMH	Exoskeleton + Squatting	5.5	33	5.67	34
	Dynamic MMH	Exoskeleton + Freestyle	6.33	38	5.33	32
Limit/Interference		Exoskeleton + Bending	5.17	31	5.17	31
		Exoskeleton + Squatting	6	36	5	32
	Static	Exoskeleton + Bending	6.83	41	5.33	32
	MMH	Exoskeleton + Squatting	4.83	29	5	30
Effectiveness	Dynamic MMH	Exoskeleton + Freestyle	6.83	41	5.67	34
		Exoskeleton + Bending	6.67	40	6.17	37
		Exoskeleton + Squatting	7.17	43	5.33	32
	Static	Exoskeleton + Bending	7.17	43	5.83	35
	MMH	Exoskeleton + Squatting	5.83	35	4.67	28

Category	Trial type	Question	Average response (%)	
Dynamic MMH		Overall feeling	moderate	
		Level of heat or humidity	17 (hot/humidity	
		Suitability for long-term use	83 (yes)	
	Exoskeleton + Freestyle	Did Exo make you use different posture?	75 (yes)	
		Your typical posture for lifting (Bending or Squatting)	86 (Squatting	
		Which posture do you think will work better with the exoskeleton?	59 (Squatting)	
	Exoskeleton + Bending	Overall feeling	Low-to-moderat	
-	Exoskeleton + Squatting	Overall feeling	Moderate	
	Quarall dunamia	Preferred posture for Dynamic MMH tasks (Bending or Squatting)	79 (Squatting)	
	Overall dynamic	Would you use the exoskeleton for dynamic MMH in overall?	71 (yes)	
Static MMH	Exoskeleton + Bending	Overall feeling	Low-to-moderat	
	Exoskeleton + Squatting	Overall feeling	Low-to-moderat	
	Overall static	Your preferred posture for static MMH tasks (Bending or Squatting)	33 (Squatting)	

Table 3 Participants' responses to usability questions

Table 4 The results of all MMH scenarios

Response type	Metric	Combined bending	Combined squatting	Combined all MMH	Combined (No-Exo)
	RPE	3.33	3.67	3.43	3.13
Usability responses	Fit/comfort	5.75	5.83	5.92	-
	Limit/Interference	5.63	5.21	5.5	-
	Effectiveness	6.46	5.75	6.13	-
	Knee	2.3	4	3.12	3.29
	Upper leg	2.9	3.53	3.11	2.5
LODs of body parts	Arm	0	2	1.1	1
	Shoulder	1.16	1	1.47	1.25
	Lower back	2.81	2	2.61	2.71
	Chest	3.25	3	3.23	0

8- Figures

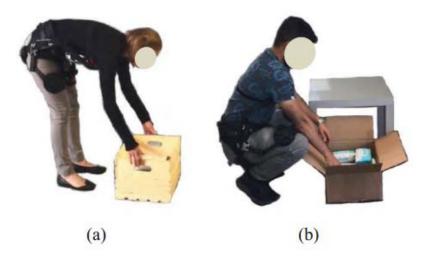


Fig. 1 Experiment Setup: (a) dynamic MMH, bending with exoskeleton, (b) static MMH, squatting with exoskelton

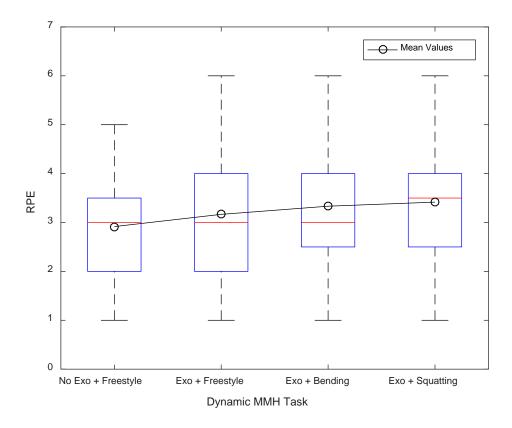


Fig. 2 Reported RPE for dynamic MMH. Results are presented for different postures, with or without wearing the exoskeleton.

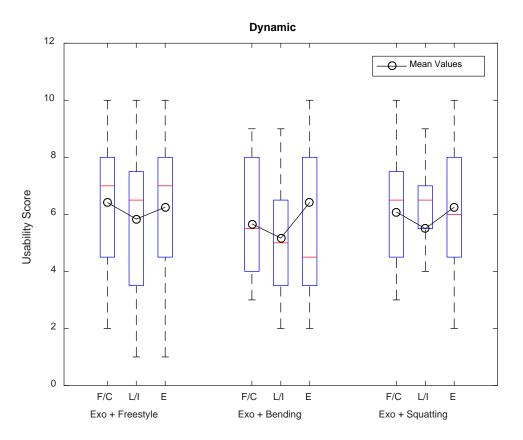


Fig. 3 Reported usability (F/C: Fit/Comfort, L/I: Limit/Interference, E: Effectiveness) of Exoskeletons for dynamic MMH. Results are presented for different postures, with or without wearing the exoskeleton.

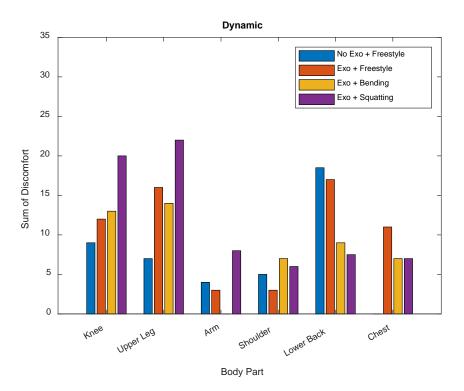


Fig. 4 Perceived discomfort of body parts for dynamic MMH. Results are presented for different postures, with or without wearing the exoskeleton.

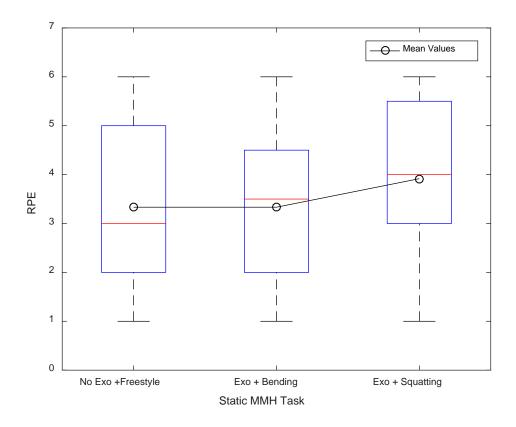


Fig. 5 Reported RPE for static MMH. Results are presented for different postures, with or without wearing the exoskeleton.

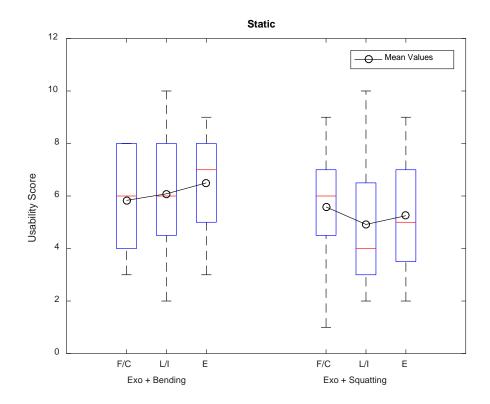


Fig. 6 Reported usability (F/C: Fit/Comfort, L/I: Limit/Interference, E: Effectiveness) of exoskeletons for static MMH in different postures.

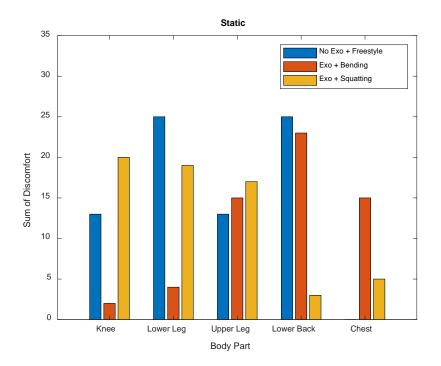


Fig. 7 Perceived discomfort of body parts for static MMH in different postures.

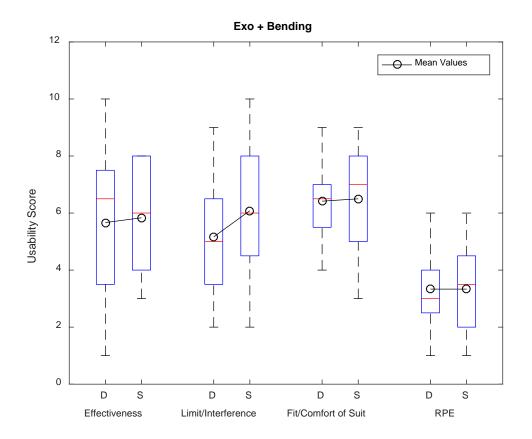


Fig. 8 Comparison of exoskeleton's usability between static (S) and dynamic (D) task scenarios for bending posture.

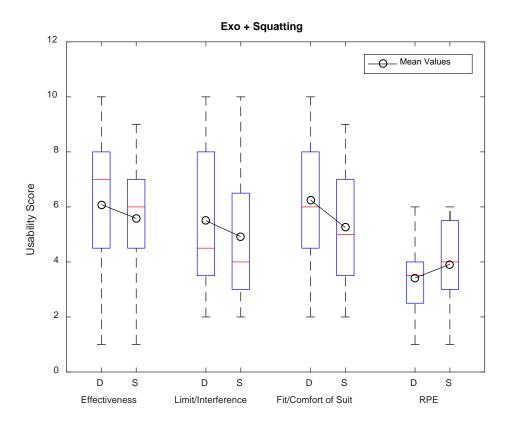


Fig. 9 Comparison of exoskeleton's usability between static (S) and dynamic (D) scenarios for squatting posture.

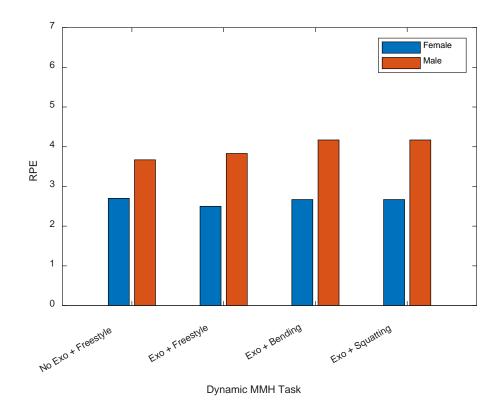


Fig. 10 RPE comparison between male and female participants for dynamic scenarios

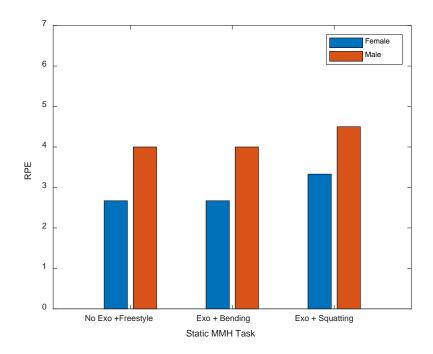


Fig. 11 RPE comparison between male and female participants for static scenarios